Robotica (2025), **43**, pp. 1572–1589
doi:10.1017/S0263574725000220

CAMBRIDGE UNIVERSITY PRESS

REVIEW ARTICLE

A scoping review on lower limb exoskeleton actuation's description and characteristics

Francesco Bettella[1], Stefano Tortora[1,2], Emanuele Menegatti[1,2], Nicola Petrone[3] and Alessandra Del Felice[1,4]

[1]Padova Neuroscience Center, University of Padova, Padova, Veneto, Italy
[2]Department of Information Engineering, University of Padova, Padova, Veneto, Italy
[3]Department of Industrial Engineering, University of Padova, Padova, Veneto, Italy
[4]Department of Neuroscience, Section of Neurology, University of Padova, Padova, Veneto, Italy
Corresponding author: Stefano Tortora; Email: stefano.tortora@unipd.it

Received: 25 April 2024; **Revised:** 31 October 2024; **Accepted:** 29 December 2024; **First published online:** 18 March 2025

Keywords: actuation; exoskeleton; robotics; parameters; motor; reducer

Abstract

Robotic lower limb exoskeletons are wearable devices designed to augment human motor functions and enhance physical capabilities mostly adopted in healthcare and rehabilitation. The field is strongly dominated by rigid exoskeletons driven by electromagnetic actuators constituted by electrical motors, gearboxes, and cylinders. This review focuses on the design and specifications of the actuation systems of lower limb exoskeletons, with the ultimate goal of providing reporting guidelines to allow for full reproducibility. For each paper, we assessed the quality and completeness of technical characteristics with two *ad hoc* rating scales for motors and reducers; we extracted the main parameters of the actuation unit and a quantitative analysis of the mechanical characteristics of the individual components was carried out considering the exoskeleton application. Overall, we observed a lack of details in reporting on actuation systems equipped on exoskeletons. To overcome this limitation, herein we conclude by proposing a data form and a checklist to provide researchers with a common approach in reporting the mechanical characteristics of the actuation unit of their lower limb exoskeletons. We believe that the convergence of exoskeletons' literature toward a clearer standardization of design and reporting will boost the development of this technology and its diffusion outside the laboratory.

1. Introduction

Lower limb exoskeletons are heterogeneous devices that differ based on their application and costs. Their scope is to enhance/restore mobility, and on these grounds, they have been mainly deployed in rehabilitation [1, 2] or as walking assistive devices outside the clinical settings. Other applications have been military [3] or human augmentation [4].

Despite the recent advances of soft robotic solutions [5], the field of lower limb exoskeletons for medical applications is still strongly dominated by rigid exoskeletons driven by electromagnetic actuators composed by electrical motors, gearboxes, and cylinders. Currently, a large variety of designs of lower limb exoskeletons for gait rehabilitation or assistance have been proposed both in the literature and on the market. However, there is an overall lack of detailed information and description of the actuation systems equipped on these devices (e.g., motor type and performance, characteristics of the transmission). Indeed, commercial exoskeleton datasheets do often not contain details about the mechanical characteristics of the actuation unit. In addition, this information is also generally overlooked in the academic literature and by previous reviews. This variety and lack of information result in two major drawbacks: i) it does not allow a complete reproducibility of the proposed devices by other research groups and

© The Author(s), 2025. Published by Cambridge University Press. This is an Open Access article, distributed under the terms of the Creative Commons Attribution licence (https://creativecommons.org/licenses/by/4.0/), which permits unrestricted re-use, distribution and reproduction, provided the original article is properly cited.

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

ii) it prevents the identification of standards and commonalities between different designs, leading to heterogeneous solutions and difficulty of comparison.

For this reason, this review focuses on the design of the actuation systems of rigid exoskeletons equipped with electromechanical/electromagnetic actuation and the description of their characteristics. Indeed, the inclusion of additional exoskeletal systems (e.g., cable-driven exosuits) would have lead to the inclusion of mechanical components and transmission technologies with critically different requirements and characteristics, limiting the thoroughness of the comparison. Thus, we decided to include in this study only rigid exoskeletons for lower limb to have a more homogeneous analysis focused on the most used and diffused category of exoskeletons. The aim is twofold (i) review the overall quality of the description of the actuation unit as reported in the various papers, highlighting the shortcomings and providing guidelines for the reporting to allow the full reproducibility of the exoskeleton's actuation units and (ii) provide a quantitative comparison of the actuation technologies and their parameters to identify standards and common characteristics among a variety of different lower limb exoskeletons.

2. Related work

Previous reviews focused on actuation methodologies of lower limb powered exoskeletons. The work published by Wang et al. [6] reported an overview of rehabilitation exoskeletons based on ergonomic design, actuation, perception, control, and validation. In particular, it describes the different types of actuation systems, highlighting the operating principles and the main advantages and disadvantages in their application, quoting some existing robots, but without reporting technical details. In the review by Plaza et al. [7], the aim was to describe the state of the art in the field of commercial medical exoskeletons, analyzing their properties, with respect to their clinical application. The authors reported only general characteristics of the systems, the walking speed, and the joints peak torque of 13 different exoskeletons. Mathew et al. [8] analyzed the technological advancements in signal sensing, actuation, control, and training methods in exoskeletons for rehabilitation, including those for lower and upper limbs. In particular, they highlighted the critical issues in designing the actuation unit using different technologies, generally describing only the type of the actuation solution and suggesting future trends in this field. Hussain et al. [9] focused on materials, actuation, and manufacturing in lower limb exoskeleton and provided a qualitative description of different actuation methods adopted by various commercial robots. Tiboni et al. [10] proposed a wide study on the world of exoskeletons investigating methods and solutions for exoskeleton design, actuation, and sensors. They conducted a statistical analysis to study the distribution of different solutions concerning the device purpose, body part to which the device is dedicated, operation mode, and design methods. In particular, the type of actuation and sensing are analyzed in detail, highlighting the main statistical trends in their development, but no technical details on the solutions are provided. The more complete technical review on lower limb exoskeletons' actuation is represented by the work of Sanchez-Villamañan et al. [11]. In their work, they reviewed 52 lower limb wearable exoskeletons. They collected data into standardized data sheets on actuation, structure, and interface attachment components. The aspects of the different solutions were highlighted creating a set of data sheets that contain the technical characteristics of the reviewed devices. However, their work focused only on exoskeletons equipped with compliant actuators, discarding all the works adopting traditional actuation solutions (e.g., DC motor with harmonic drives) that represent the majority of the exoskeletons currently present in the literature and on the market. The current review differs from these works as we aim at providing guidelines and reporting a checklist to allow reproducibility of the actuation unit of rigid lower limb exoskeletons. In addition, we completed an in-depth revision on the specific technical parameters of each component (i.e., motor, transmission) in existing systems to find trends that can be useful to build an initial standardization [12].

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

Table I. *Data extraction form used for the technical parameters collection.*

Exoskeleton							
Authors	Year	doi	DOF	Application	Name		
Motor							
Type	Brand	Model	Voltage [V]	Max power [W]	Nom torque [Nm]	Nom speed [rpm]	Weight [kg]
Reducer							
Type	Brand	Model	Ratio	Max repeated peak torque [Nm]	Max momentary peak torque [Nm]	Max input speed [rpm]	Weight [kg]

3. Materials and methods

3.1. Inclusion criteria

Inclusion criteria were as follows: (i) peer-reviewed papers, (ii) in English language, regarding (iii) rigid bilateral lower limb exoskeletons, (iv) simultaneously powered at hips and knees joints, and (v) equipped with electromechanical/electromagnetic actuation systems. Exclusion criteria were virtual models and simulations. Articles, conference papers, and book chapters were considered eligible, whereas reviews and conference abstracts were excluded. Patent descriptions were also excluded because they do not report technical details of the components aiming, instead, at protecting designs or solutions. Exoskeletons for military and industrial applications were also excluded from this study.

3.2. Articles selection

The following databases were used: Scopus and PubMed. The search string was modeled using the AND and OR Boolean operators, which correspond respectively to the algebraic intersection and union, as follows: *exoskeleton AND ((lower AND limb) OR walk*) AND (active OR powered) AND (motor OR actuator OR adapter OR design)*. The search string and databases used in the study were chosen with help from an expert researcher and agreed among the authors. Figure 1(a) reports the Preferred Reporting Items for Systematic Review and Meta-Analysis extension for Scoping Reviews [13] flow chart. A total of 1692 papers published until January 2025 were identified. Duplicates were excluded utilizing the Zotero software: 1383 articles remained for title screening. Subsequently, based on title screening, the papers out of topic or inclusion criteria were excluded. A total of 266 articles underwent abstract screening. Hundred and twenty-four papers remained for full-text analysis. During both title and abstract screening, if a paper did not meet the agreement of all the investigators about the inclusion/exclusion criteria, it was moved to the next stage. One investigator (FB) carried out the process, and the papers were cross-checked by two experienced reviewers (ST, NP). A fourth evaluator (EM) reviewed the papers in case of discrepancies with other evaluators.

3.3. Data extraction process

A data extraction process was applied for each article that met the inclusion criteria ($N = 66$). The distribution over the years of the papers included in this study is reported in Figure 1(b). A standardized form was developed to extract data from the selected papers, reported in Table I. The extraction form contained the following data: 1) authors and year of publication, 2) the digital object identifier (DOI) number of the publication, 3) degrees of freedom defined as the number of actuated joints, and 4) exoskeleton's application (e.g., rehabilitative or assistive) and name if present. If the application was not explicitly mentioned or easily identifiable from the article, we classified the device as "prototype". In addition, specific technical characteristics of the actuation system were extracted for each exoskeleton joint

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

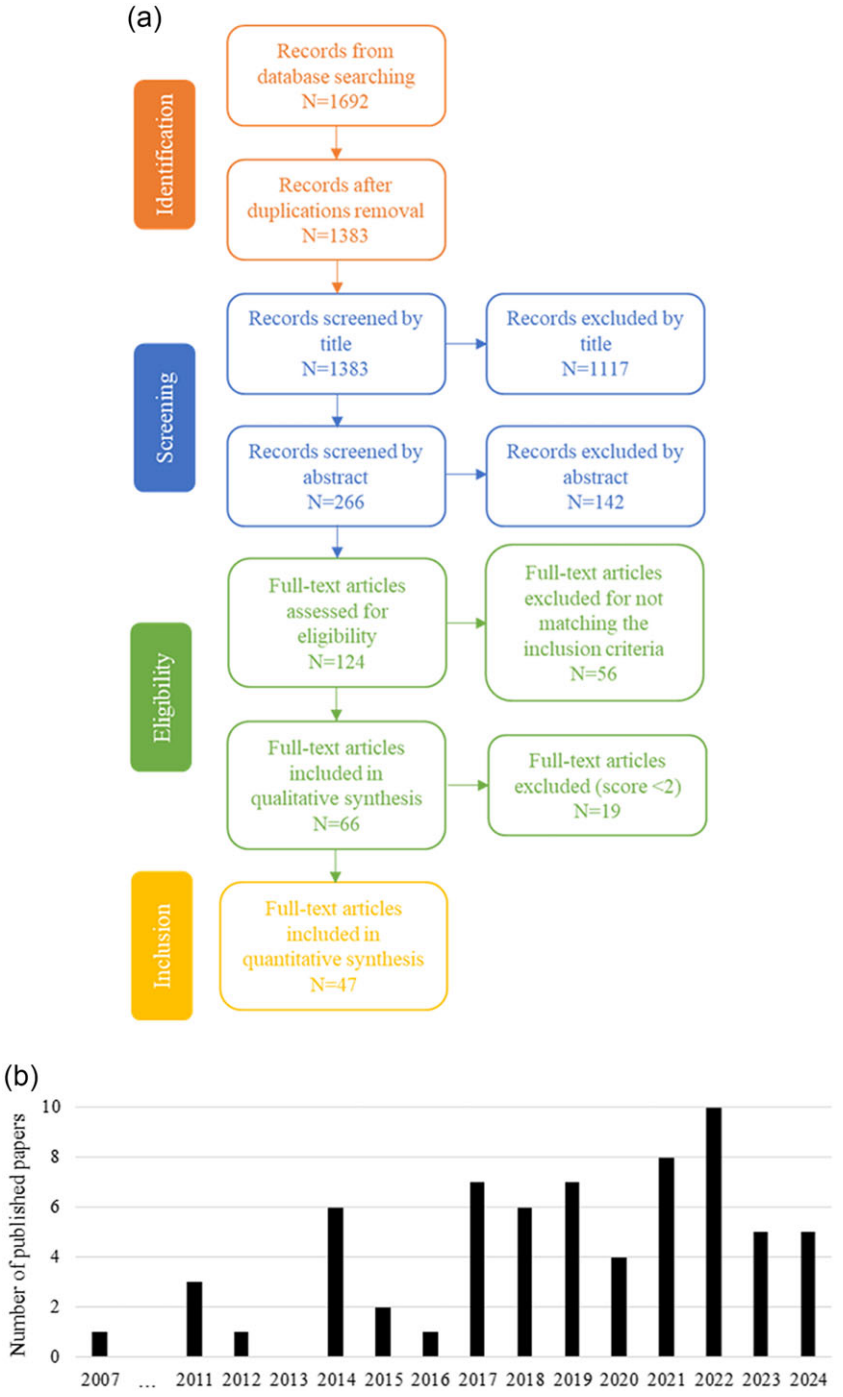


Figure 1. *(a) PRISMA flow of the articles selection process. (b) Bar chart displaying the number of papers included in the study, (b) distribution over the years of the papers included in the study.*

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

Table II. *Rating scales used for the quality assessment of exoskeleton's actuation.*

Rating	Motor	Reducer
1	No information	No information
2	Only type indicated	Only type indicated
3	Brand and model	Only reduction ratio
4	Brand, model and power or voltage	Type and reduction ratio
5	Complete description	Complete description

(i.e., hip and knee). In particular, the following parameters were taken into consideration, separated by system component:

- *Motor*: type, brand, model, voltage, maximum power, nominal torque, maximum speed, weight;
- *Reducer*: type, brand, model, reduction ratio, maximum repeated peak torque, maximum momentary peak torque, maximum input speed, maximum average input speed, and weight.

To extract the technical data of each component, the following process was used. First, the values explicitly reported in the papers were transcribed. If these values were not provided, further online searches were conducted. In particular, if the article provided sufficient details to unequivocally determine the specific motors and reducers, the mechanical characteristics of interest were obtained from the catalog of the producers. To unequivocally identify the motor from the catalogs, the minimum information necessary to be indicated in the article are the brand, the model, the voltage, and the wattage. When not provided, a standard voltage value of 24 V for motor control was hypothesized [14–19]. Instead for the reducers, the brand, the model, and the reduction ratio are necessary. In case an information is missing and not identifiable from the catalogs, the information is marked as "not defined" (i.e., "N/D"). Not having the internal structure of the reducers, being commercial products, we included the characteristics available common to all the reducers. Another technical parameter to investigate should be the size of the components. However, volume is a difficult information to find as it is not explicitly indicated in the catalogs. It should be calculated from the external dimensions of the components, but too few values for making any comparison were available. Moreover, the overall external dimensions depend not only on the size of each component but also on the geometry of the assembly. This makes the comparison between the exoskeletons impossible.

3.4. Quality assessment

A quality assessment was conducted for each article to investigate the quality of the articles on reporting the technical description of the actuation units based on the data extracted in the previous stage. The quality assessment was designed according to the approach used in previously published systematical and/or meta-analysis review [20, 21] and customized to our needs and application. Thus, two *ad hoc* rating scales were arranged, one for the motor description and one for the reducer description as reported in Table II. The rating was initially performed by two investigators (FB, ST) independently. Then, a cross-check by a third investigator (NP) was performed for the articles for which there were discrepancies between the ratings of the two investigators. The rating was defined based on the presence or absence in the article of the motor and reducer information collected in the data extraction form. The rating scores were set from 1 up to 5. A score of 1 indicates the lack of actuation description or the absence of any technical parameters for the motor and/or reducer. If only the motor type is mentioned (e.g., Brushed or Brushless DC motor), a score of 2 was assigned to the article. If the article provides the brand and the model of the motor used, thus allowing a search of the average motor characteristics from the producer catalog, the article was assessed with a quality score of 3. If also the power or the driving voltage of the motor is specified, the article is rated as 4 since this information allows us to extract the exact motor

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

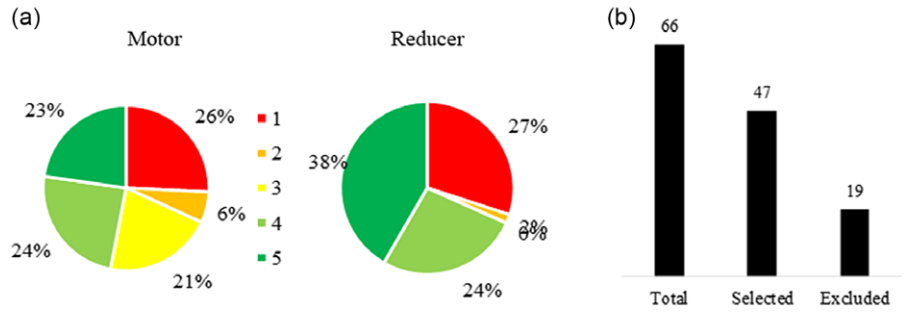


Figure 2. *(a) Results of parameters description rating for motors on the left and reducers on the right. Scores are from 1 up to 5 where 1 indicates that no information about the component is provided and 5 represents a complete description. (b) Paper selection: a total of 66 articles met the inclusion criteria. Only the papers that obtained a score ≥ 3 up to 5 in at least one proposed rating scale on motors and reducers were selected for the following quantitative analysis (N = 47). The remaining 19 articles whose scoring was ≤ 2 in both rating scales were excluded from the subsequent analysis.*

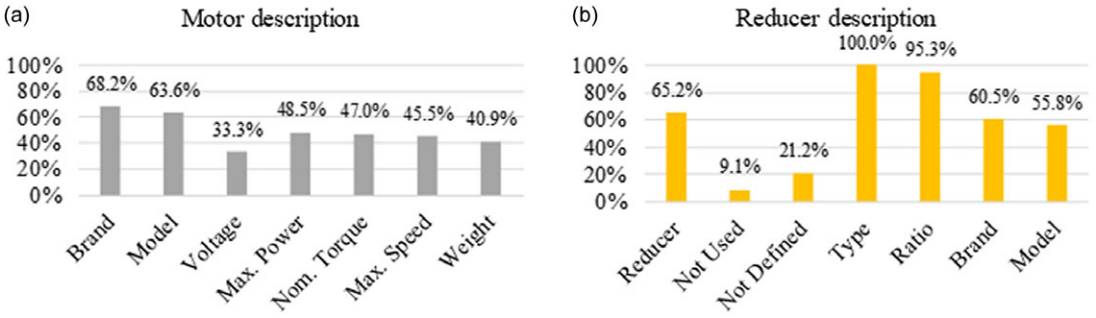


Figure 3. *Percentage of reviewed papers sufficiently reporting the technical parameters on fundamental characteristics of (a) motors and (b) reducers. A parameter was considered as sufficiently reported if explicitly indicated by the authors or if it can be unequivocally extracted from external sources, i.e., catalogs.*

characteristics from the catalogs. For the reducer, the score of 2 and 3 indicates that the article reports either the reducer type (e.g., harmonic drive or planetary gearbox) only or the reduction ratio only. If both type and reduction ratio are reported, the article is rated as 4. A score of 5 in the two scales indicates that the article fully describes the technical characteristics of both the motor and the reducer without the need for an additional search in the catalogs. Only studies rated 4 or 5 can be considered reproducible.

4. Results

4.1. Qualitative analysis

Of the 124 papers selected for full-text analysis, 56 did not meet the inclusion criteria. Figure 2(a) shows the distribution of scores associated to the papers included in full-text qualitative analysis ($N = 66$) (Figure 2b). Of note, 21 (32%) of the considered full papers do not provide sufficient information on the motor and 19 (29%) on the reducer. In particular, regarding motor description, 17 papers (26%) do not provide any detail (rating score 1) and 4 of them (6%) provide information only on the type (rating score 2). Moreover, 18 of them (28%) do not provide any information on the reduction system (rating score 1) and 1 of them (2%) indicate only the type. Only 15 (23%) and 25 (38%) out of 66 reviewed papers provided full details about the motor and reducer, respectively.

To provide a clearer picture on the completeness of the technical information reported in the literature, Figure 3 shows the percentage of papers reporting each of the information and parameters

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

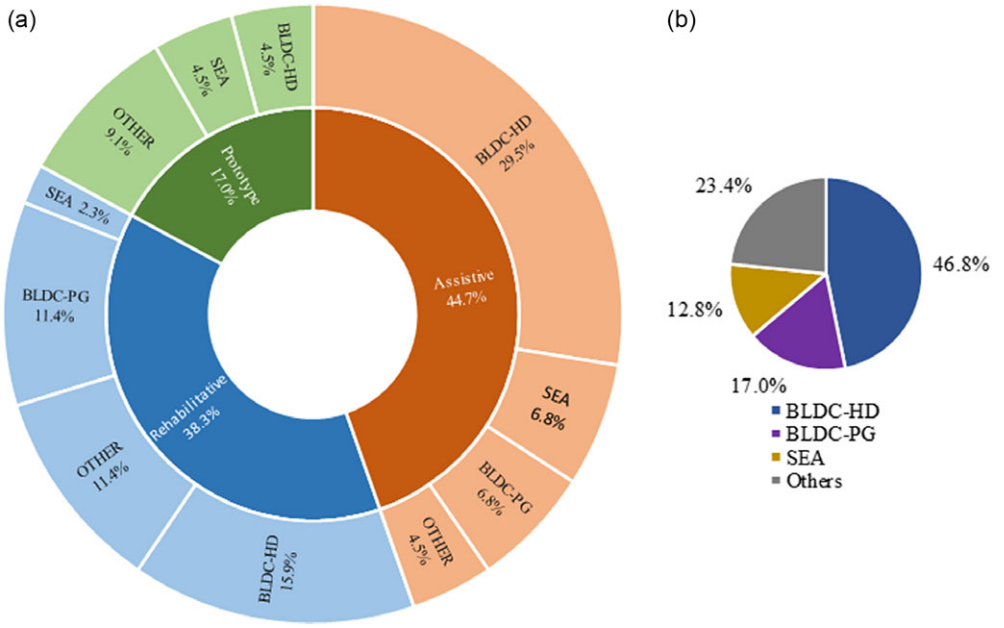


Figure 4. *(a) The distribution of exoskeletons' applications is reported in the inner circles. Exoskeletons with no specified use are defined as "Prototype". For each application, the percentage of actuation unit solutions is reported. The main three types are brushless DC motor in combination with a harmonic drive (BLDC-HD), brushless DC motor coupled with a planetary gearbox (BLDC-PG), and serial elastic actuator (SEA). Combinations of different solutions or personalized designs are indicated as "Other". (b) Global distribution of type of actuation unit among all the analyzed exoskeletons.*

considered in the data form, for both motors (Figure 3a) and reducers (Figure 3b). Overall, 68.2% of the papers ($N = 45$) declared at least the brand of the motor, while 63.6% ($N = 42$) indicated also the model. However, only 33.3% ($N = 22$) indicated the supply voltage and 48.5% ($N = 32$) the power of the motor. The lack of these information hampered the search for other parameters not expressly indicated in the paper from external sources such as catalogs. It was thus possible to identify the nominal torque, maximum speed, and weight values in less than 50% of the reviewed articles. For what concerns the reducers, 69.7% of the exoskeletons ($N = 46$) use a reducer for both hip and knee joints, and all of these (46 out of 46) indicate the type. The 95.7% of papers declared the reduction ratio, and the 58.7% indicated also the brand of the reducer. However, only the 54.3% provided also the model. Exceptions are represented by 6 exoskeletons (9.1%) that do not use any reducer in their actuation system and 14 (21.2%) do not provide any information on the reducer equipped on the exoskeleton.

Based on this qualitative assessment, we decided that those papers providing insufficient information (rating score ≤ 2) on both motor and reducer of the actuated exoskeleton joints were excluded from the subsequent analysis, maintaining only the papers that obtained a score ≥ 3 up to 5 in at least one proposed rating scale on motors and reducer description.

4.2. Quantitative analysis

The following quantitative analysis considers only the 46 papers that provide sufficient information on either the motor or the reducer, as selected in the qualitative analysis. In Figure 4(a), the classification of the actuation systems divided by the exoskeleton's application is shown. Assistive application is the most frequent ($N = 21$, 44.7%), followed by rehabilitative ones ($N = 18$, 38.3%). Exoskeletons with no specified use are defined as "Prototype" ($N = 8$, 17.0%). Actuation units present different solutions.

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

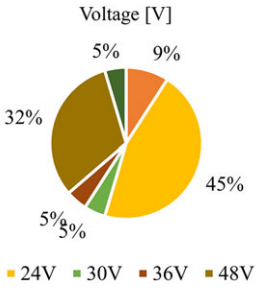


Figure 5. *Percentage distribution of motors' power supply voltage reported in the articles. Only values expressly provided by authors are included.*

Assistive robots are mainly characterized by the use of a brushless DC Motor in combination with a harmonic drive (BLDC-HD), while rehabilitative ones and prototypes have a more homogeneous distribution among the technologies. Globally, the BLDC-HD solution is the most adopted ($N = 22$, 46.8%) as shown in Figure 4(b). The reason for this prevalence is likely its back-drivability, allowing movement even if the motors are powered off [19] and reducing errors due to backlash. On the other hand, 17.0% of the papers ($N = 8$) used a brushless DC motor coupled with a planetary gearbox (BLDC-PG) and 12.8% ($N = 6$) adopted a serial elastic actuator (SEA) system for force transmission. SEA is composed by an electric motor in combination with compliant elements to reduce shocks during gait phases, often associated with a reducer, allowing a more biofidelic behavior of the joints. Moreover, there are other particular systems that are a combination of the previous ones or a personalized design for a specific application. In detail, only CUHK-EXO by Bing et al. [22] and the exoskeleton by Ghezal et al. [23] adopted brushed DC motors for their actuation units. The first one is in combination with a planetary gearbox, and the second is part of a SEA system. Furthermore, MLLRE exoskeleton by Guo et al. [24] was composed by a body weight support and a four-bar linkage moved by an AC servo motor. In the exoskeletons presented in Liu et al. [25] and Bergmann et al. [26], a variable stiffness actuator (VSA) was used. VSA is an independent-setup, consisting of a double-actuation system that can perform the joint torque/position and stiffness control task independently [27]. A windshield wiper motor, composed by an electric motor attached to a worm gear, which transmits the force to a rod, was used in [28]. I-EXO [29] and WSE [30] exoskeletons adopted a brushless DC motor and a servomotor, respectively, without mentioning the presence of a reducer. The exoskeleton designed by Fang et al. [31] adopted a stepper motor for the leg motion. Other works used compliant elements in combination with the motor which have the purpose of absorbing impacts and shocks on the joints [32–34]. These different solutions will be indicated as "Others" in the following analysis.

4.3. Actuation characteristics

In the following sections, the parameters of the different exoskeletons' actuation technology are reported and analyzed.

4.3.1. Motors

Figure 5 shows the distribution of motor supply voltage values used in the reviewed articles that expressly indicate this information. As expected, the widely used solution involved a voltage of 24 V.

In Figure 6, the values of maximum power, nominal torque, maximum speed, and weight of the motors are reported with the corresponding standard deviations. For each parameter, the overall mean and the averages of the three most used actuation types (brushless DC motor coupled with harmonic drive – BLDC-HD, brushless DC motor coupled with planetary gearbox – BLDC-PG, serial elastic actuator – SEA) were calculated. It can be seen that the solutions combining the planetary gearbox adopt motors

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

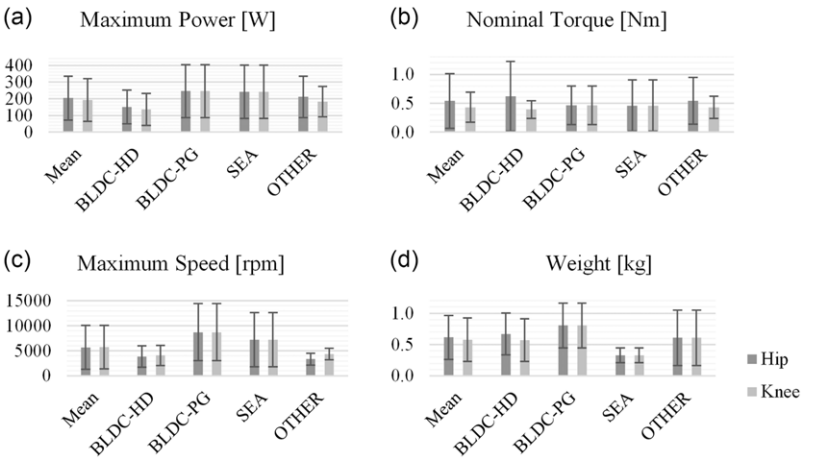


Figure 6. *Technical parameters of motors are reported for hip (dark gray) and knee (light gray) joints. In detail, (a) maximum power, (b) nominal torque, (c) maximum speed, and (d) weight of the electrical motor. For each parameter, the overall mean among all the systems and the averages of systems divided by their actuation unit type are reported. The considered actuation types are: brushless DC motor with a harmonic drive (BLDC-HD), brushless DC motor with a planetary gearbox (BLDC-PG), serial elastic actuator (SEA), and personalized designs (OTHER).*

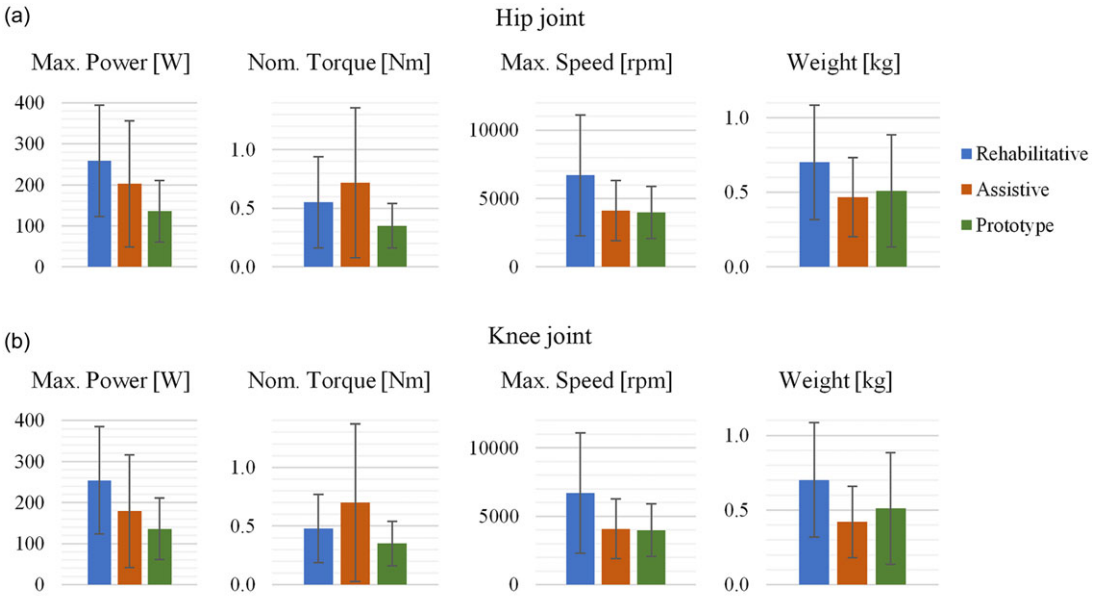


Figure 7. *Average values of the motor's parameters for the hip and knee joints based on exoskeletons' application.*

with greater power and speed than the solutions that couple a harmonic drive and SEA. The same trend can be found in the motor weight, with SEA solutions adopting lighter motors with lower torque and higher speed.

We analyzed the motor parameters based on the applications of the exoskeletons, as shown in Figure 7 reporting values both for the hip and knee joints' actuation. Overall, we can notice that rehabilitative devices adopt more powerful and heavy motors on average than the other applications.

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

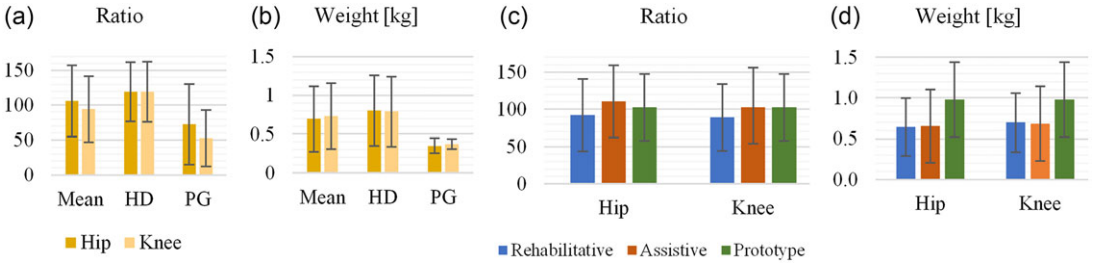


Figure 8. *(a) Reduction ratio and (b) weight of reducers are reported. The overall mean among all the systems adopting a reducer and the averages of systems adopting harmonic drive (HD) and planetary gearbox (PG), both for hip and knee joints, are indicated. (c) The average values of hip and knee joints reduction ratio and (d) reducer weight based on exoskeletons' application are reported.*

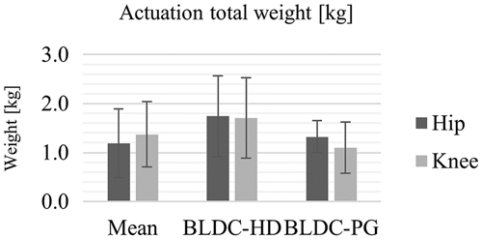


Figure 9. *Joint actuation total weight composed by the sum of the motor and the reducer is reported, for hip and knee joints. Only systems reporting the weights of both motor and reducer are included (N = 14) and the overall mean among all the systems and the averages of systems adopting harmonic drive (BLDC-HD) and planetary gearbox (BLDC-PG) were calculated.*

4.3.2. Reducers

In Figure 8(a), we report the values of the reduction ratio of the reducers for the hip and knee joints with the corresponding standard deviations. Figure 8(b) reports the values of weight. For each parameter, the overall average values and the means of the two most used solutions (harmonic drive and planetary gearbox) were calculated. In systems that use a harmonic drive, the reduction ratio is almost double compared to applications with planetary reducers. However, the average weight of the analyzed planetary gearboxes is half compared to that of the harmonic drives (Figure 8b). Moreover, as Figure 8(c) shows, exoskeletons for assistive application on average adopt a greater reduction ratio than the rehabilitative ones, even if the average reducer weight is almost the same (Figure 8d).

4.3.3. Global actuation unit

Observing the total weight of the joint actuation shown in Figure 9, composed by the weight of the motor and of the reducer, it is important to notice that the solutions with planetary gearbox are almost 50% lighter than the solutions using a harmonic drive.

Figure 10 shows the values of the maximum power and the nominal torque of the motor and the reduction ratio of each exoskeleton. The graphs report the types of the actuation system, represented with different symbols, and the application of the exoskeleton, depicted with different colors. As previously reported, we could not include all exoskeletons due to missing details of motors, reducers, or both. The missing values were therefore indicated with N/D. All systems that use SEA (indicated with squares) do not use reducers, except two systems that use custom SEA in combination with a harmonic drive [35, 36]. We performed a linear regression between the extracted values to analyze if there is a relationship between the power of the motors used and the reduction ratio chosen. The dotted lines indicate the linear regressions for each exoskeleton group divided according to their application. Overall, we identified a negative trend in the regression lines in all the conditions, except for the "prototype" group in the

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

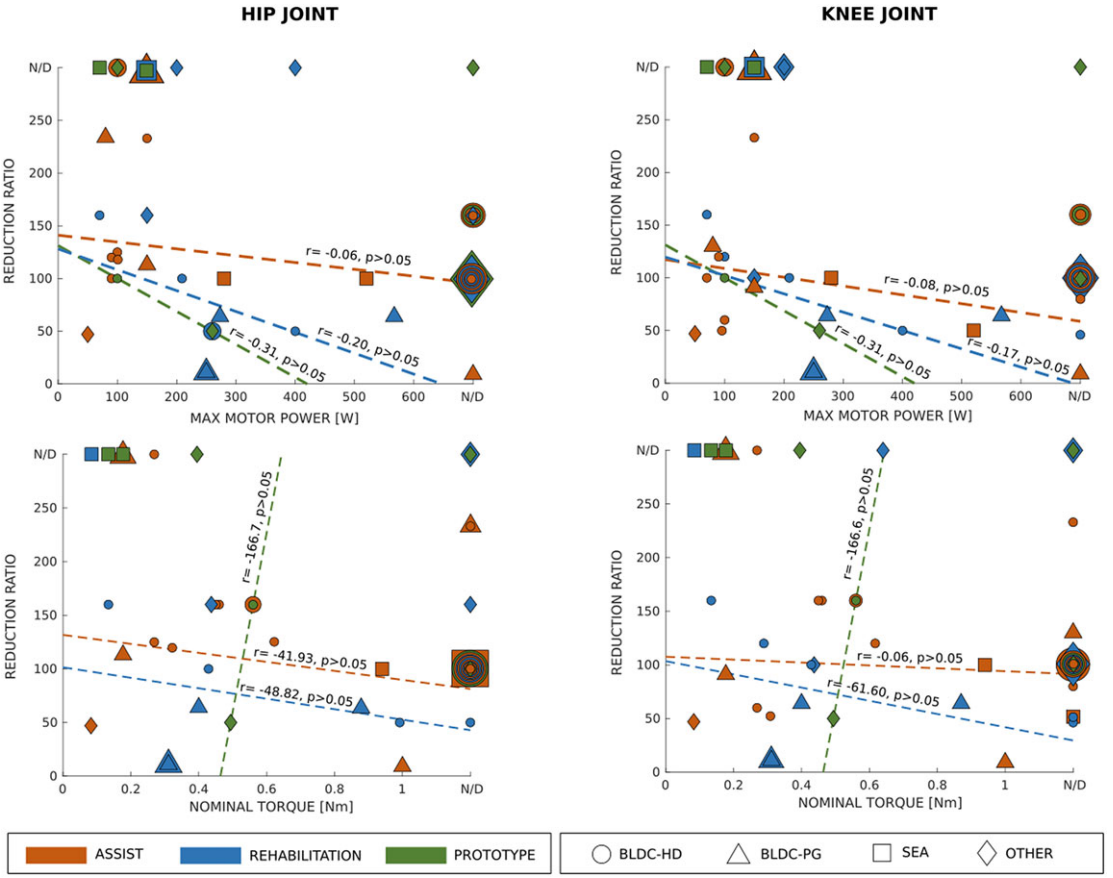


Figure 10. *The relationships between the reduction ratio and the motor size are reported for bot hip and knee joints, considering respectively the maximum motor power (top) and the nominal torque (bottom). The exoskeleton applications are indicated with different colors, and the types of the actuation system are indicated with different symbols. The dotted lines indicate the linear regressions for the exoskeletons grouped by their application. Values that are not reported in the manuscript nor identifiable from cataloges are marked as N/D.*

reduction ratio vs. nominal torque analysis. This indicates that on average there is a trade-off between the motors' power and the ratio of the transmission – i.e., exoskeletons equipped with more powerful motors employ reducers with lower reduction ratios. This feature is more marked in rehabilitative exoskeletons, although without a statistical significance ($p > 0.05$). In particular, exoskeletons that use a brushless DC motor and a harmonic drive tend to use motors with lower power and nominal torque coupled with higher reduction ratios, compared to solutions adopting planetary reducers, as shown also in Figure 6(a) and Figure 8(a).

5. Discussion

5.1. Actuation technologies

Accurate selection and sizing of actuation are crucial steps in designing exoskeletons to achieve lightweight and transparent systems. In this review, we define "actuation" as the subsystem responsible for generating mechanical power at the joint level of the exoskeleton. Therefore, the following discussion

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

will encompass considerations related to motor characteristics and transmission design solutions, contextualized according to the identified exoskeleton application. First of all, it is possible to observe that there is an important heterogeneity in many parameters. This variability can be explained by the fact that the solutions adopted by the authors are often very different because there are big differences also in the structure of the exoskeleton. This changes the requirements between one device and another and involves the use of components, although of the same type, very different from each other. Analyzing these data, we wanted to study whether there were trends associated with the various types of components used.

Our review demonstrates that brushless DC motors are the most used electric actuators. Only CUHK-EXO by Bing et al. [22] and the exoskeleton by Ghezal et al. [23] adopted brushed DC motors for their actuation units. Specifically, brushless motors in combination with a harmonic drive represent the most used solution. Indeed, despite the relatively low cost with respect to brushless motors, brushed DC solutions are being progressively abandoned due to their higher rotor inertia, higher friction, higher electromagnetic noise, and lower power-to-weight ratio [37, 38]. The use of harmonic drive allows for higher reduction ratios than the solution with planetary reducers. Consequently, the motor can have lower torque and minor powers. The reduced weight of a smaller motor is compensated by the increased weight of the harmonic reducer (Figure 9). On the other hand, using a lower-powered motor allows for the adoption of a smaller battery pack while maintaining the same usage duration.

The use of SEA is a more recent solution and allows for more biofidelic behavior of the joints in the contact instants. They require the presence of compliant elements in series with the motors, but involve a more complex design and often custom-made torsional springs [35, 36]. This aspect could be problematic in the commercialization phase of the exoskeleton, as the use of non-standard components could lead to an important increase of the exoskeleton cost [39]. On average, exoskeletons for rehabilitation use adopt more powerful motors and, in general, a greater variety of solutions than those for assistive use. This might be explained in light of the severity and variety of mobility disorders of people with disabilities undergoing physical rehabilitation (e.g., stroke [40], cerebral palsy [41], spinal cord injury [42], orthopedic post-surgery patients [43]), and the necessity to accommodate different types of motor training [1]. On the other hand, users of assistive systems are usually people with residual walking capabilities, such as elderly people [32], who therefore require only partial support during the activities of daily living. The trend in exoskeleton's applications is to inversely relate the maximum power of the motor to the reduction ratio of the reducer, when present, usually in favor of low-power motors coupled with higher reduction ratio ≥ 100 (Figure 10). In fact, assistive devices are used mainly outside clinical environments and therefore have requirements of portability, weight and cost. The BLDC-HD system is the best at meeting these requirements. As a result, given the increased application on the market, research is more focused on rehabilitation devices, while assistive exoskeletons rely on implementation on a more robust and stable technology. Research focuses more on wearability and human–machine interface. However, there are some exceptions such as the Symbitron [36], an assistive exoskeleton that moves on inclined surfaces (e.g., slopes and stairs). Therefore, it adopts more powerful actuation units (520W brushless DC motor plus a harmonic drive with ratio 100 for the hip and 50 for the knee and a set of torsional springs). Another system, the LOPES exoskeleton for rehabilitation use has a support structure and adopts SEA with a combination of cable-driven actuation with high-power servomotors, 567W, coupled with planetary gearboxes of 64 ratio [44]. In general, from the results obtained in this study, it is possible to observe that, despite the trends highlighted, there are different technologies for the actuation of rigid exoskeletons for lower limbs. This is also demonstrated by the high heterogeneity in many parameters, as resulted from the standard deviation calculation. This variability can be explained by the fact that the solutions adopted by the authors are often very different, due to the variety of mobility disorders and disabilities of users. This leads to big differences also in the structure of the exoskeletons. In our opinion, it is important to define a standardization and indications of reporting technical details, to support the development of these systems in the coming years. In view of the increasingly widespread use of these technologies, extending it to everyday life and outdoor environments, it is essential to improve the autonomy and transportability of systems, as well as increasing performance and reliability. Therefore,

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

Table III. *Checklist of the fundamental set of technical details to report in the actuation unit description.*

Motor		
Type	A1	Indicate the type of the motor
Brand	A2	Indicate the brand of the motor
Model	A3	Indicate the model of the motor
Voltage	A4	Indicate the supply voltage of the motor
Max power	A5	Indicate the maximum power of the motor
Nom torque	A6	Indicate the nominal torque of the motor
Nom speed	A7	Indicate the nominal speed of the motor
Weight	A8	Indicate the weight of the motor
Reducer		
Type	R1	Indicate the type of the reducer
Brand	R2	Indicate the brand of the reducer
Model	R3	Indicate the model of the reducer
Ratio	R4	Indicate the reduction ratio of the reducer
Max repeated peak torque	R5	Indicate the maximum repeated peak torque of the reducer
Max momentary peak torque	R6	Indicate the maximum momentary peak torque of the reducer
Max input speed	R7	Indicate the maximum input speed of the reducer
Weight	R8	Indicate the weight of the reducer

we believe that there will be three main directions in research. First, reducing weight and external dimensions can allow a less demanding and more natural use of the system. This is a key aspect to improve performances and rehabilitation and assistive results and increase the versatility of systems. Surely having smaller motors will help to reduce the weight and adopting reducers with high reduction ratio as harmonic drives or other technologically advanced reducers will also allow them to contain the external dimensions. This trend will also lead to the application of smaller and more powerful batteries that can increase the autonomy of the use of the exoskeletons, which is the second most critical development. It is important to improve this characteristic to guarantee a sufficient usage time, especially in outdoor environments. The third research direction will improve ergonomics and user comfort and in this field the use of SEA is emerging in recent years. It guarantees greater comfort for the user especially during the contact phase. One future development should be to optimize the design of components to simplify the construction and lower the costs, allowing a wider application.

5.2. Quality of actuation description

Another objective of this review was to define if the parameters and characteristics of the actuation units of the exoskeletons' joints are sufficiently described to allow the reproducibility of the system. The aim, being this a scoping review, was not to provide a complete technical analysis of all the exoskeleton systems, for which we refer to [10, 11]. It was mainly to identify pitfalls in the mechanical description of the exoskeleton's actuation units and propose a potential standardization for the reporting [12]. In particular, herein we focused on papers describing exoskeletons equipped with electromagnetic/electromechanical actuation, excluding other types of common actuation systems in lower limb exoskeleton (e.g., pneumatic or hydraulic actuation). We took this decision for two main reasons: first, to allow a more homogeneous definition and clearer comparison of the most relevant parameters describing the actuation unit; second, electromechanical actuations represent the most widely used solutions for exoskeletons [10] as they provide enough power for the full actuation of the user's lower limbs while having higher benefits in terms of weight and dimensions compared to the other solutions [45, 46].

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

Overall, we observed a lack of technical information across the reviewed literature. Only 47% of included papers report sufficient information and technical data of the motors used for the actuation systems. Indeed, 32% do not provide any technical detail beyond the type of component used and the remaining provide partial but insufficient data. Reducers are better described than motors due to their minor complexity and variety. However, 30% of reviewed works do not provide any description also of reducers. The technical description of actuation is tendentially overlooked. Indeed, most of the works focused more on the aspects of sensing and control [47–53], or on the gait pattern generation [54] without entering in the details of the exoskeleton technical characteristics. Others focus on specific aspects of the system, e.g., the human–exoskeleton interface [55] or the experimental evaluation of the system on the end-users [56]. Another category includes works reporting on uncommon solutions with complex construction demands, which focus on the description of the structure design and the mechanisms while neglecting details of the actuation unit [57–61]. Specifically, information that are often missing are the selected voltage supply for running the exoskeleton and the power of the motor. Even if the brand and the model are provided, the lack of these details prevents the identification of the motor and the parameters of interest (e.g., weight, nominal and peak torque, and maximum speed) from the catalogs. Nevertheless, the analysis of the papers providing the voltage supply ($N = 21$) revealed a clear trend toward the usage of 24 V power supply, supporting our initial choice of assuming a 24 V supply whenever not stated.

In view of the above results, we aim at providing a checklist of the minimum fundamental set of technical details to be provided to ensure reproducibility for lower limb powered exoskeletons, reported in Table III. It has to be combined with the data extraction form used in this review and reported in Table I. In addition, a full list of the papers included in the review is provided as Supplementary Material to simplify the comparison between newly developed systems and the state of the art. If a commercial motor from a specific producer is used, only the first data in the list must be provided. In particular, providing type, brand, model, supply voltage, and wattage allows to obtain the other values from external sources (i.e., catalogs). On the other hand, if the system is equipped with a custom-made motor, it is necessary to indicate at least power supply voltage, maximum power, nominal torque, peak torque, nominal speed, and weight. In this way, it is possible to search for an equivalent commercial motor or develop a custom-made one with the same mechanical characteristics as those used in the exoskeleton that is reproduced. Similarly, for commercial reducers, it is necessary to report the type, brand, model, and transmission ratio to obtain the other values from external sources. Otherwise, the parameters description of custom-made reducers must be provided, indicating the reduction ratio, transmissible nominal torque, transmissible peak torque, maximum input speed, and weight. When writing papers regarding the exoskeleton actuation system, it would be important to follow the guidelines reported in this checklist and at the same time fill in the data extraction form to ensure to provide all the information necessary for the reproducibility of the actuation units.

6. Conclusions

This review was systematically conducted by applying the PRISMA statements to collect all the papers regarding rigid bilateral lower limbs exoskeleton, powered simultaneously at hip and knee joints, equipped with electromechanical/electromagnetic actuation system. The first aim was to focus on the design of the actuation systems and the quality of the description of their characteristics to ensure reproducibility. Subsequently, a quantitative comparison of the reported actuation technologies was conducted to identify standards and common characteristics among different lower limb exoskeletons. An overall lack of detailed information and description of the actuation systems resulted. Despite this lack of technical details, we observed trends in the technical characteristics of the actuation units' components, such as a trade-off with motor power and reduction ratio according to the exoskeleton application. These information can be used to build a more complete and organic standardization. The guidelines and checklists proposed in this review are an initial contribution in this direction.

Author contributions. FB, ST, NP, and ADF conceived and designed the study. FB conducted data gathering. ST performed statistical analyses. FB and ST wrote the article. EM, NP, and ADF supervised the work and reviewed the article.

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

Financial support. The work was supported by Italian Minister for Education (MUR), under REACT-EU PON "Ricerca e Innovazione." This paper was developed within the project funded by Next Generation EU– "Age-It–Ageing well in an ageing society" project (PE0000015), National Recovery and Resilience Plan (NRRP)–PE8–Mission 4, C2, Intervention 1.3". The views and opinions expressed are only those of the authors and do not necessarily reflect those of the European Union or the European Commission. Neither the European Union nor the European Commission can be held responsible for them.

Competing interests. No conflicts of interest exist.

Ethical approval. Not applicable.

Supplementary material. The supplementary material for this article can be found at https://doi.org/10.1017/S0263574725000220.

References

[1] D. Shi, W. Zhang, W. Zhang and X. Ding, "A review on lower limb rehabilitation exoskeleton robots," *CJME* **32**(1), 1–11 (2019).
[2] J. A. de la Tejera, R. Bustamante-Bello, R. A. Ramirez-Mendoza and J. Izquierdo-Reyes, "Systematic review of exoskeletons towards a general categorization model proposal," *Appl. Sci.* **11**(1), 76 (2021). Number: 1 Publisher: Multidisciplinary Digital Publishing Institute.
[3] S. Yu, C. Han and I. Cho, "Design considerations of a lower limb exoskeleton system to assist walking and load-carrying of infantry soldiers," *Appl. Bionics Biomech.* **11**(3), 119–134 (2014).
[4] H. Kazerooni, "Exoskeletons for Human Power Augmentation," 2005 IEEE/RSJ International Conference on Intelligent Robots and Systems, IEEE, New York City, US (2005) pp. 3459–3464.
[5] A. F. P. Vidal, J. Y. R. Morales, G. O. Torres, F. d. J. Sorcia Vázquez, A. C. Rojas, J. A. B. Mendoza and J. C. R. Cerda, "Soft exoskeletons: Development, requirements, and challenges of the last decade, "*Actuators*, **10**, 166 (2021). MDPI.
[6] T. Wang, B. Zhang, C. Liu, T. Liu, Y. Han, S. Wang, J. P. Ferreira, W. Dong and X. Zhang, "A review on the rehabilitation exoskeletons for the lower limbs of the elderly and the disabled," *Electronics* **11**(3), 388 (2022).
[7] A. Plaza, M. Hernandez, G. Puyuelo, E. Garces and E. Garcia, "Lower-limb medical and rehabilitation exoskeletons: A review of the current designs," *R-BME* **16**, 278–291 (2021).
[8] M. Mathew, M. J. Thomas, M. Navaneeth, S. Sulaiman, A. Amudhan and A. Sudheer, "A systematic review of technological advancements in signal sensing, actuation, control and training methods in robotic exoskeletons for rehabilitation," (2022). Industrial Robot: the international journal of robotics research and application,(ahead-of-print)
[9] F. Hussain, R. Goecke and M. Mohammadian, "Exoskeleton robots for lower limb assistance: A review of materials, actuation, and manufacturing methods," *Proc Inst Mech Eng H.* **235**(12), 1375–1385 (2021).
[10] M. Tiboni, A. Borboni, F. Vérité, C. Bregoli and C. Amici, "Sensors and actuation technologies in exoskeletons: A review," *Sensors* **22**(3), 884 (2022).
[11] M. d. C. Sanchez-Villamañan, J. Gonzalez-Vargas, D. Torricelli, J. C. Moreno and J. L. Pons, "Compliant lower limb exoskeletons: A comprehensive review on mechanical design principles," *J Neuroeng Rehabil* **16**(1), 1–16 (2019).
[12] D. Torricelli, J. Gonzalez-Vargas, J. F. Veneman, K. Mombaur, N. Tsagarakis, A. J. Del-Ama, A. Gil-Agudo, J. C. Moreno and J. L. Pons, "Benchmarking bipedal locomotion: A unified scheme for humanoids, wearable robots, and humans," *IEEE Robot Autom Mag* **22**(3), 103–115 (2015).
[13] A. C. Tricco, E. Lillie, W. Zarin, K. K. O'Brien, H. Colquhoun, D. Levac, D. Moher, M. D. J. Peters, T. Horsley, L. Weeks, S. Hempel, E. A. Akl, C. Chang, J. McGowan, L. Stewart, L. Hartling, A. Aldcroft, M. G. Wilson, C. Garritty, S. Lewin, C. M. Godfrey, M. T. Macdonald, E. V. Langlois, K. Soares-Weiser, J. Moriarty, T. Clifford, Ö. Tunçalp and S. E. Straus, "Prisma extension for scoping reviews (prisma-scr): Checklist and explanation," *Ann Intern Med.* **169**(7), 467–473 (2018).
[14] R. M. Andrade and P. Bonato, "The role played by mass, friction, and inertia on the driving torques of lower-limb gait training exoskeletons," *IEEE Trans Med Robot Bionics* **3**(1), 125–136 (2021).
[15] O. Baser, H. Kizilhan and E. Kilic, "Biomimetic compliant lower limb exoskeleton (biocomex) and its experimental evaluation," *J Braz Soc Mech Sci* **41**(5), 1–15 (2019).
[16] B. Chen, C.-H. Zhong, X. Zhao, H. Ma, X. Guan, X. Li, F.-Y. Liang, J. C. Y. Cheng, L. Qin, S.-W. Law and W.-H. Liao, "A wearable exoskeleton suit for motion assistance to paralysed patients," *J Orthop Translat* **11**, 7–18 (2017).
[17] H. Choi, "Assistance of a person with muscular weakness using a joint-torque-assisting exoskeletal robot," *Appl. Sci.* **11**(7), 3114 (2021).
[18] S. Christensen, S. Bai, S. Rafique, M. Isaksson, L. O'Sullivan, V. Power and G. S. Virk, "Axo-suit-a modular full-body exoskeleton for physical assistance, "Mechanism Design for Robotics: Proceedings of the 4th IFToMM Symposium on Mechanism Design for Robotics, Springer, New York City, US (2019) pp. 443–450.
[19] S. Christensen, S. Rafique and S. Bai, "Design of a powered full-body exoskeleton for physical assistance of elderly people," *Int J Adv Robot Syst* **18**(6), 17298814211053534 (2021).
[20] F. A. Storm, A. Cesareo, G. Reni and E. Biffi, "Wearable inertial sensors to assess gait during the 6-minute walk test: A systematic review," *Sensors* **20**(9), 2660 (2020).

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

[21] M. Rubega, R. Di Marco, M. Zampini, E. Formaggio, E. Menegatti, P. Bonato, S. Masiero and A. D. Felice, "Muscular and cortical activation during dynamic and static balance in the elderly: A scoping review," *Aging Brain* **1**, 100013 (2021).

[22] B. Chen, C.-H. Zhong, H. Ma, X. Guan, L.-Y. Qin, K.-M. Chan, S.-W. Law, L. Qin and W.-H. Liao, "Sit-to-stand and stand-to-sit assistance for paraplegic patients with cuhk-exo exoskeleton," *Robotica* **36**(4), 535–551 (2018).

[23] M. Ghezal, M. Guiatni, I. Boussioud and C. S. Renane, "Design and robust control of a 2 dofs lower limb exoskeleton, " 2018 International Conference on Communications and Electrical Engineering (ICCEE), IEEE, New York City, US (2018) pp. 1–6.

[24] Z. Guo, H. Yu and Y. H. Yin, "Developing a mobile lower limb robotic exoskeleton for gait rehabilitation," *J. Med. Devices* **8**(4), 044503 (2014).

[25] L. Liu, S. Leonhardt, C. Ngo and B. J. Misgeld, "Impedance-controlled variable stiffness actuator for lower limb robot applications," *IEEE Trans Autom Sci Eng* **17**(2), 991–1004 (2019).

[26] L. Bergmann, O. Lück, D. Voss, P. Buschermöhle, L. Liu, S. Leonhardt and C. Ngo, "Lower limb exoskeleton with compliant actuators: Design, modeling, and human torque estimation," *IEEE/ASME Trans Mechatron* **28**(2), 758–769 (2022).

[27] L. Liu, S. Leonhardt and B. J. Misgeld, "Experimental validation of a torque-controlled variable stiffness actuator tuned by gain scheduling," *IEEE/ASME Trans Mechatron* **23**(5), 2109–2120 (2018).

[28] Y. Taza-Aquino and D. Huamanchahua, "Mechanical and electronic design of a prototype of a modular exoskeleton for lower-limbs, " IEEE International IOT, Electronics and Mechatronics Conference (IEMTRONICS) 2022, IEEE, New York City, US (2022) pp. 1–6.

[29] J. Wang, D. Wu, W. Dong and Y. Gao, "A control strategy for squat assistance of lower limb exoskeleton with back sensing, " In, 2022 IEEE International Conference on Mechatronics and Automation (ICMA), IEEE, New York City, US (2022) pp. 1312–1317.

[30] Ü. Önen, F. M. Botsalı, M. Kalyoncu, M. Tınkır, N. Yılmaz and Y. Şahin, "Design and actuator selection of a lower extremity exoskeleton," *IEEE/ASME Trans Mechatron* **19**(2), 623–632 (2013).

[31] Y. Fang, B. Hou, X. Wu, Y. Wang, K. Osawa and E. Tanaka, "A stepper motor-powered lower limb exoskeleton with multiple assistance functions for daily use by the elderly," *JRM* **35**(3), 601–611 (2023).

[32] B. Brackx, J. Geeroms, J. Vantilt, V. Grosu, K. Junius, H. Cuypers, B. Vanderborght and D. Lefeber, "Design of a modular add-on compliant actuator to convert an orthosis into an assistive exoskeleton, "5th IEEE RAS/EMBS International Conference on Biomedical Robotics and Biomechatronics, IEEE, New York City, US (2014) pp. 485–490.

[33] C. Huang, W. Chen, J. Liu and J. Zhang, "Design of a compliant joint actuator for lower-limb exoskeleton robot," 2017, 12th IEEE Conference on Industrial Electronics and Applications (ICIEA), IEEE, New York City, US (2017) pp. 1522–1527

[34] B. Penzlin, L. Bergmann, Y. Li, L. Ji, S. Leonhardt and C. Ngo, "Design and first operation of an active lower limb exoskeleton with parallel elastic actuation, "*Actuators*, **10**, 75 (2021).

[35] M. C. Yildirim, A. T. Kansizoglu, S. Emre, M. Derman, S. Coruk, A. F. Soliman, P. Sendur and B. Ugurlu, "Co-ex: A torque-controllable lower body exoskeleton for dependable human-robot co-existence, " 2019 IEEE 16th International Conference on Rehabilitation Robotics (ICORR), IEEE (2019) pp. 605–610

[36] C. Meijneke, G. van Oort, V. Sluiter, E. van Asseldonk, N. L. Tagliamonte, F. Tamburella, I. Pisotta, M. Masciullo, M. Arquilla, M. Molinari, A. R. Wu, F. Dzeladini, A. J. Ijspeert and H. van der Kooij, "Symbitron exoskeleton: Design, control, and evaluation of a modular exoskeleton for incomplete and complete spinal cord injured individuals," *IEEE Trans Neural Syst Rehabil Eng* **29**, 330–339 (2021).

[37] D. G. Dorrell, M.-F. Hsieh and A. M. Knight, "Alternative rotor designs for high performance brushless permanent magnet machines for hybrid electric vehicles," *IEEE Trans Magn*. **48**(2), 835–838 (2012).

[38] G. Qiao, G. Liu, Z. Shi, Y. Wang, S. Ma and T. C. Lim, "A review of electromechanical actuators for more/all electric aircraft systems," *Proc Inst Mech Eng C J Mech Eng Sci* **232**(22), 4128–4151 (2018).

[39] F. Ferrati, R. Bortoletto, E. Menegatti and E. Pagello, "Socio-Economic Impact of Medical Lower-Limb Exoskeletons," 2013 IEEE workshop on advanced robotics and its social impacts, IEEE, New York City, US (2013) pp. 19–26.

[40] F. Ferrati, R. Bortoletto, E. Menegatti and E. Pagello, "Socio-Economic Impact of Medical Lower-Limb Exoskeletons," **In:** In, *2013 IEEE Workshop On Advanced Robotics and Its Social Impacts*, (IEEE, (2013) pp. 19–26.

[41] S. A. Murray, K. H. Ha, C. Hartigan and M. Goldfarb, "An assistive control approach for a lower-limb exoskeleton to facilitate recovery of walking following stroke," *IEEE Trans Neural Syst Rehabil Eng* **23**(3), 441–449 (2014).

[42] Z. F. Lerner, D. L. Damiano and T. C. Bulea, "A lower-extremity exoskeleton improves knee extension in children with crouch gait from cerebral palsy," *Sci Transl Med* **9**(404), eaam9145 (2017).

[43] H. S. F. White, S. Hayes and M. White, "The effect of using a powered exoskeleton training programme on joint range of motion on spinal injured individuals: A pilot study," *Int. J. Phys. Ther. Rehabil* **1**(2), 1–5 (2015).

[44] D.-q. Wan, Y.-m. Xu, Y.-h. Bai and Y.-h. Yin, "R318application of lower limb exoskeletons rehabilitation robots in rehabilitation treatment of activity limited knee joint," *Chinese Journal of Tissue Engineering Research* **16**(4), 597 (2012).

[45] J. F. Veneman, R. Kruidhof, E. E. Hekman, R. Ekkelenkamp, E. H. Van Asseldonk and H. Van Der Kooij, "Design and evaluation of the lopes exoskeleton robot for interactive gait rehabilitation," *IEEE Trans Neural Syst Rehabil Eng* **15**(3), 379–386 (2007).

[46] P. Agarwal and A. D. Deshpande, "Exoskeletons: State-of-the-art design challenges and future directions," **In:** *Human Performance Optimization: The Science and Ethics of Enhancing Human Capabilities* (Michael D. Matthews, and David M. Schnyer, eds.), (Online edn, Oxford Academic, New York, 2019).

[47] P. Maciejasz, J. Eschweiler, K. Gerlach-Hahn, A. Jansen-Troy and S. Leonhardt, "A survey on robotic devices for upper limb rehabilitation," *J Neuroeng Rehabil* **11**(1), 1–29 (2014).

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

[48] W. Banchadit, A. Temram, T. Sukwan, P. Owatchaiyapong and J. Suthakorn, "Design and implementation of a new motorized-mechanical exoskeleton based on cga patternized control," *2012 IEEE International Conference on Robotics and Biomimetics (ROBIO)*, IEEE, New York City, US (2012) pp. 1668–1673.
[49] A. Ortlieb, M. Bouri, R. Baud and H. Bleuler, "An assistive lower limb exoskeleton for people with neurological gait disorders, "2017 International Conference on Rehabilitation Robotics (ICORR), IEEE, New York City, US (2017) pp. 441–446
[50] L. I. Minchala, A. J. Velasco, J. M. Blandin, F. Astudillo-Salinas and A. Vazquez-Rodas,"Low cost lower limb exoskeleton for assisting gait rehabilitation: Design and evaluation, "Proceedings of the 2019 3rd International Conference on Automation, Control and Robots 2019, New York City, US (2019) pp. 55–60.
[51] W. Sanngoen, S. Nillnawarad and S. Patchim, "Design and development of low-cost assistive device for lower limb exoskeleton robot, "2017, 10th International Conference on Human System Interactions (HSI), IEEE, New York City, US (2017) pp. 148–153
[52] K. Seo, K. Kim, Y. J. Park, J.-K. Cho, J. Lee, B. Choi, B. Lim, Y. Lee and Y. Shim, "Adaptive oscillator-based control for active lower-limb exoskeleton and its metabolic impact, "2018 IEEE International Conference on Robotics and Automation (ICRA), IEEE, New York City, US (2018) pp. 6752–6758
[53] A. K. Tanyildizi, O. Yakut, B. Taşar and A. B. Tatar, "Control of twin-double pendulum lower extremity exoskeleton system with fuzzy logic control method," *Neural Comput Appl* **33**(13), 8089–8103 (2021).
[54] A. R. Wu, F. Dzeladini, T. J. Brug, F. Tamburella, N. L. Tagliamonte, E. H. Van Asseldonk, H. Van Der Kooij and A. J. Ijspeert, "An adaptive neuromuscular controller for assistive lower-limb exoskeletons: A preliminary study on subjects with spinal cord injury," *Front. neurorobot.* **11**, 30 (2017).
[55] Z. Yan, N. Li, X. Long, H. Ren and X. Wu,"Bionic mechanical design and stair ascending/descending gait planning of a lower-limb exoskeleton robot, "2018 IEEE International Conference on Cyborg and Bionic Systems (CBS), IEEE, New York City, US (2018) pp. 155–160.
[56] L. Levesque, S. Pardoel, Z. Lovrenovic and M. Doumit, "Experimental comfort assessment of an active exoskeleton interface,"2017 IEEE International Symposium on Robotics and Intelligent Sensors (IRIS), IEEE, New York City, US (2017) pp. 38–43.
[57] R. J. Farris, H. A. Quintero and M. Goldfarb, "Preliminary evaluation of a powered lower limb orthosis to aid walking in paraplegic individuals," *IEEE Trans Neural Syst Rehabil Eng* **19**(6), 652–659 (2011).
[58] S. Hasan and A. K. Dhingra, "Biomechanical design and control of an eight dof human lower extremity rehabilitation exoskeleton robot," *RICO* **7**, 100107 (2022).
[59] R. Ranaweera, W. Jayasiri, W. Tharaka, J. Gunasiri, R. Gopura, T. Jayawardena and G. Mann, "Anthro-x: Anthropomorphic lower extremity exoskeleton robot for power assistance," 4th International Conference on Control, Automation and Robotics (ICCAR) 2018, IEEE, New York City, US (2018) pp. 82–87.
[60] Q. Shi, X. Zhang, J. Chen and Y. Chen, "Design on mechanism of lower limb rehabilitation robot based on new body weight support (bws) system,"2014 IEEE International Conference on Information and Automation (ICIA), IEEE, New York City, US (2014) pp. 108–112.
[61] S. Zhou, Z. Chen, W. Song, S. Zhu, L. Jin and J. Gu, "Design and gait realization of power-assisted lower limbs exoskeleton, " IEEE International Conference on Cybernetics and Intelligent Systems (CIS) and IEEE Conference on Robotics, Automation and Mechatronics (RAM) 2019, IEEE, New York City, US (2019) pp. 101–106.
[62] Y. Zhu, J. Yang, H. Jin, X. Zang and J. Zhao, "Design and evaluation of a parallel-series elastic actuator for lower limb exoskeletons," 2014 IEEE International Conference on Robotics and Automation (ICRA), IEEE, New York City, US (2014) pp. 1335–1340.
[63] D. Tian, W. Li, J. Li, F. Li, Z. Chen, Y. He, J. Sun and X. Wu, "Self-balancing exoskeleton robots designed to facilitate multiple rehabilitation training movements," *IEEE Trans Neural Syst Rehabil Eng* **32**, 293–303 (2024).
[64] A. F. Soliman, S. Coruk, M. C. Yildirim, D. Ugur, S. C. Cevik, B. Ozkaynak, P. Sendur and B. Ugurlu, "Design, development, and control for the self-stabilizing bipedal exoskeleton prototype co-ex," *IEEE ASME Trans Mechatron* **30**(1), 458–468 (2024).
[65] S. Qiu, Z. Pei, J. Shi, X. Zhang, C. Wang and Z. Tang, "Design-modeling and control of a novel wearable exoskeleton for lower-limb enhancement," *IEEE Robotics and Automation Letters* **9**(7), 6640–6647 (2024).
[66] X. Li, K.-Y. Wang and Z.-Y. Yang, "Design and analysis of a lower limb assistive exoskeleton robot," *Technol Health Care.* **32**, 1–15 (2024). (Preprint).
[67] L. Yu, H. Leto and S. Bai, "Design and gait control of an active lower limb exoskeleton for walking assistance," *Machines* **11**(9), 864 (2023).
[68] A. Plaza, M. Hernandez, A. Gutierrez, J. Ramos, G. Puyuelo, C. Cumplido, E. Garces, M. A. Destarac, E. Delgado and E. Garcia, "Design of a modular exoskeleton based on distributed central pattern generators," *IEEE Syst J* **17**(1), 816–827 (2022).
[69] G. Li, Z. Li, C.-Y. Su and T. Xu, "Active human-following control of an exoskeleton robot with body weight support," *IEEE Trans Cybern* **53**(11), 7367–7379 (2023).
[70] X. Gao, P. Zhang, X. Peng, J. Zhao, K. Liu, M. Miao, P. Zhao, D. Luo and Y. Li, "Autonomous motion and control of lower limb exoskeleton rehabilitation robot," *Front. bioeng. biotechnol.* **11**, 1223831 (2023).
[71] C. Changcheng, Y.-R. Li and C.-T. Chen, "Assistive mobility control of a robotic hip-knee exoskeleton for gait training," *Sensors* **22**(13), 5045 (2022).
[72] P. Huang, Z. Li, M. Zhou, X. Li and M. Cheng, "Fuzzy enhanced adaptive admittance control of a wearable walking exoskeleton with step trajectory shaping," *IEEE Trans Fuzzy Syst* **30**(6), 1541–1552 (2022).

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press

[73] C. Nesler, G. Thomas, N. Divekar, E. J. Rouse and R. D. Gregg, "Enhancing voluntary motion with modular, backdrivable, powered hip and knee orthoses," *IEEE Robot Autom Lett* **7**(3), 6155–6162 (2022).
[74] C.-T. Pan, M.-C. Lee, J.-S. Huang, C.-C. Chang, Z.-Y. Hoe and K.-M. Li, "Active assistive design and multiaxis self-tuning control of a novel lower limb rehabilitation exoskeleton," *Machines* **10**(5), 318 (2022).
[75] T. Vouga, J. Fasola, R. Baud, A. R. Manzoori, J. Pache and M. Bouri, "Twiice one powered exoskeleton: Effect of design improvements on usability in daily life as measured by the performance in the cybathlon race," *J Neuroeng Rehabil* **19**(1), 63 (2022).
[76] X. Zhou, Z. Yu, M. Wang, D. Chen and X. Ye,"Design of control system for lower limb exoskeleton robot, "8th International Conference on Control, Automation and Robotics (ICCAR) 2022, IEEE, New York City, US (2022) pp. 122–126.
[77] M. Laffranchi, S. D'Angella, C. Vassallo, C. Piezzo, M. Canepa, S. De Giuseppe, M. Di Salvo, A. Succi, S. Cappa, G. Cerruti, S. Scarpetta, L. Cavallaro, Nò Boccardo, M. D'Angelo, C. Marchese, J. A. Saglia, E. Guanziroli, G. Barresi, M. Semprini, S. Traverso, S. Maludrottu, F. Molteni, R. Sacchetti, E. Gruppioni and L. De Michieli, "User-centered design and development of the modular twin lower limb exoskeleton," *Front. neurorobot.* **15**, 709731 (2021).
[78] S. M. T. Zarandi, S. K. H. Sani, M. R. A. Tootoonchi, A. A. Tootoonchi and M.-G. Farajzadeh-D, "Design and implementation of a real-time nonlinear model predictive controller for a lower limb exoskeleton with input saturation," *Iran. J. Sci. Technol. - Trans. Electr. Eng.* **45**(1), 309–320 (2021).
[79] M. Cardona, C. E. G. Cena, F. Serrano and R. Saltaren, "Alice: Conceptual development of a lower limb exoskeleton robot driven by an on-board musculoskeletal simulator," *Sensors* **20**(3), 789 (2020).
[80] Y. Li, X. Guan, X. Han, Z. Tang, K. Meng, Z. Shi, B. Penzlin, Y. Yang, J. Ren, Z. Yang, et al., "Design and preliminary validation of a lower limb exoskeleton with compact and modular actuation," *IEEE access* **8**, 66338–66352 (2020).
[81] Y. Pirjade, D. Londhe, N. Patwardhan, A. Kotkar, T. Shelke and S. S. Ohol, "Design and fabrication of a low-cost human body lower limb exoskeleton, "2020, 6th International Conference on Mechatronics and Robotics Engineering (ICMRE), IEEE, New York City, US (2020) pp. 32–37.
[82] C.-F. Chen, Z.-J. Du, L. He, Y.-J. Shi, J.-Q. Wang, G.-Q. Xu, Y. Zhang, D.-M. Wu and W. Dong, "Development and hybrid control of an electrically actuated lower limb exoskeleton for motion assistance," *IEEE Access* **7**, 169107–169122 (2019).
[83] M. Yang, X. Wang, Z. Zhu, R. Xi and Q. Wu, "Development and control of a robotic lower limb exoskeleton for paraplegic patients," *Proc. Inst. Mech. Eng. C* **233**(3), 1087–1098 (2019).
[84] Y. He, C. Wang, N. Li, R. Fu and X. A.-L. Wu, "A novel autonomous lower extremity exoskeleton for walking assistance, "IEEE International Conference on Information and Automation (ICIA), New York City, US (2018) pp. 11–13.
[85] S. O. Schrade, K. Dätwyler, M. Stücheli, K. Studer, D.-A. Türk, M. Meboldt, R. Gassert and O. Lambercy, "Development of varileg, an exoskeleton with variable stiffness actuation: First results and user evaluation from the cybathlon 2016," *J Neuroeng Rehabil* **15**(1), 1–18 (2018).
[86] T. Vouga, R. Baud, J. Fasola, M. Bouri and H. Bleuler, "Twiice–a lightweight lower-limb exoskeleton for complete paraplegics, "2017 International Conference on Rehabilitation Robotics (ICORR), IEEE, New York City, US (2017) pp. 1639–1645.
[87] Z. Zhu, C. Jiang, X. Wang, J. Chen, L. He and Q. Wu, "Design of a Wearable Lower Limb Exoskeleton for Paralyzed Individuals, "2016, 23rd International Conference on Mechatronics and Machine Vision in Practice (M2VIP), IEEE, New York City, US (2016) pp. 1–6.
[88] H. T. Tran, H. Cheng, H. Rui, X. Lin, M. K. Duong and Q. Chen, "Evaluation of a fuzzy-based impedance control strategy on a powered lower exoskeleton," *Int J Soc Robot* **8**(1), 103–123 (2016).
[89] D. Cha, S. N. Oh, H. H. Lee, K.-S. Kim, K. I. Kim and S. Kim, "Design and evaluation of the unmanned technology research center exoskeleton implementing the precedence walking assistance mechanism," *J Electr Eng Technol* **10**(6), 2376–2383 (2015).
[90] J.-H. Park, J.-S. Lee, J.-S. Shin and B.-K. Cho, "Design of a Lower Limb Exoskeleton Including Roll Actuation to Assist Walking and Standing Up," 2015 IEEE-RAS 15th International Conference on Humanoid Robots (Humanoids), IEEE, New York City, US (2015) pp. 359–364.
[91] J. Fang, Y. Ren and D. Zhang, "A Robotic Exoskeleton for Lower Limb Rehabilitation Controlled by Central Pattern Generator," **In:** *2014 IEEE International Conference on Robotics and Biomimetics (ROBIO 2014)*, IEEE, New York City, US (2014) pp. 814–818.
[92] O. Unluhisarcikli, M. Pietrusinski, B. Weinberg, P. Bonato and C. Mavroidis, "Design and Control of a Robotic Lower Extremity Exoskeleton for Gait Rehabilitation, "RSJ International Conference on Intelligent Robots and Systems (IROS), IEEE, San Francisco, CA, USA (2011) pp. 489.
[93] P. D. Neuhaus, J. H. Noorden, T. J. Craig, T. Torres, J. Kirschbaum and J. E. Pratt, "Design and Evaluation of Mina: A Robotic Orthosis for Paraplegics, "2011 IEEE International Conference on Rehabilitation Robotics, IEEE, New York City, US (2011) pp. 1–8.
[94] P. K. Jamwal, S. Dauletbayev, D. Sagidoldin, D. Keikibayev, A. Niyetkaliyev, S. Hussain and S. K. Agrawal, "Design and transparency assessment of a gait rehabilitation robot with biomimetic knee joints," *IEEE Trans Med Robot Bionics* **7**(1), 290–302 (2025).

Cite this article: F. Bettella, S. Tortora, E. Menegatti, N. Petrone and A. Del Felice (2025). "A scoping review on lower limb exoskeleton actuation's description and characteristics", Robotica **43**, 1572–1589. https://doi.org/10.1017/S0263574725000220

https://doi.org/10.1017/S0263574725000220 Published online by Cambridge University Press